



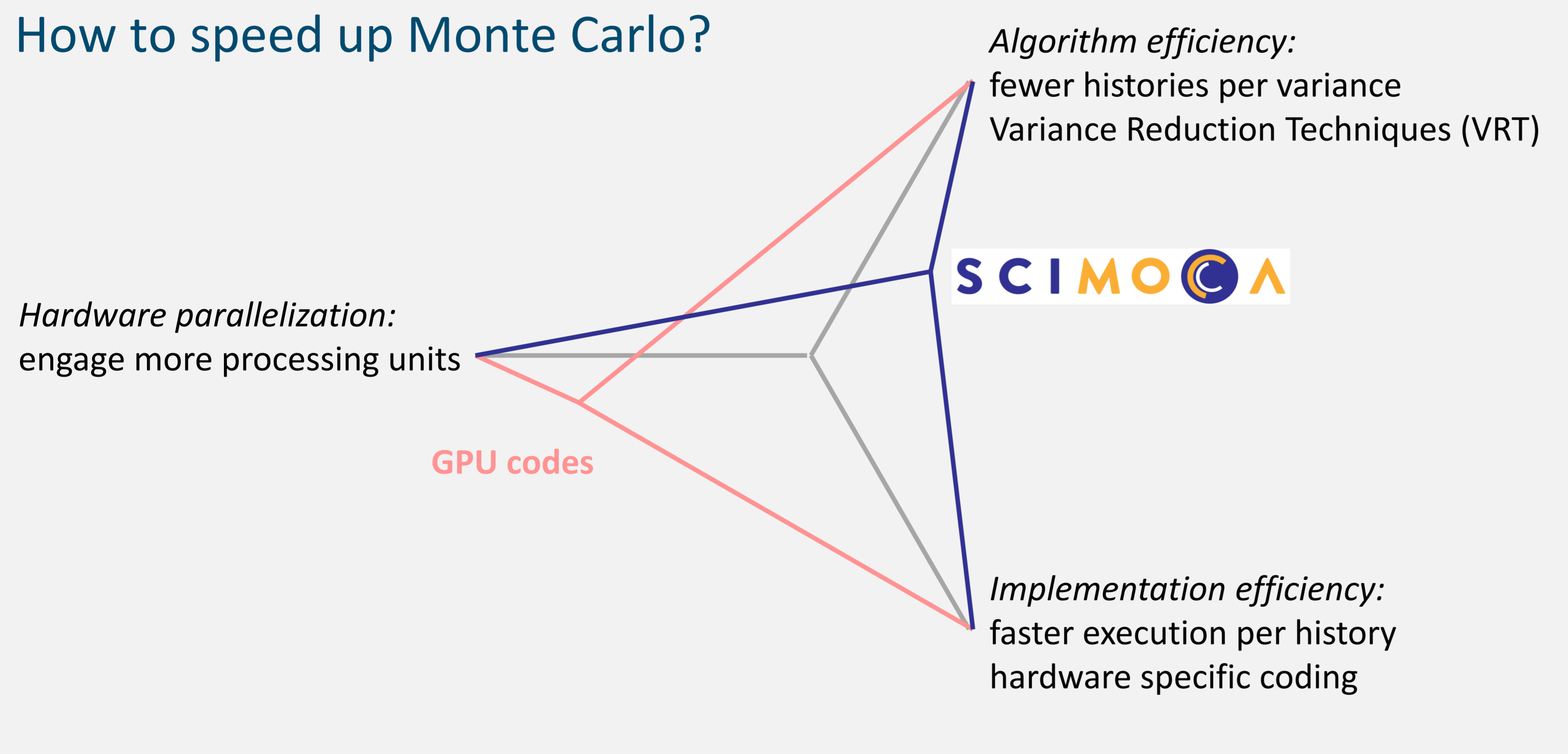
UNIVERSITÄTS
KLINIKUM
HEIDELBERG

Towards real-time Monte Carlo dose computation: muscle or brain?

M. Alber^{1,2}, N. Saito^{1,2}, M. Sohn²

¹Department of Radiation Oncology, Universitätsklinikum Heidelberg; ²DSscientific RT GmbH, Munich

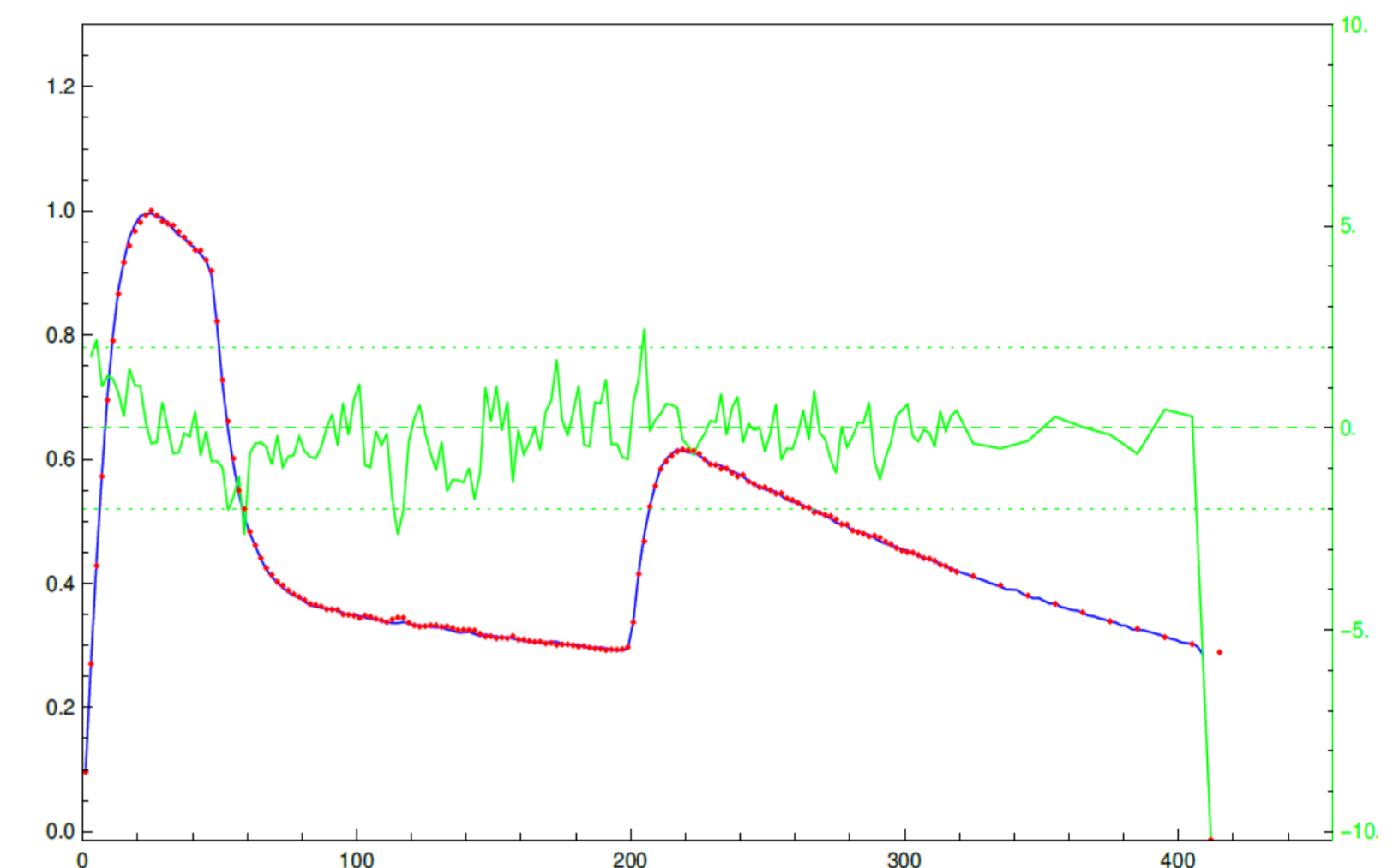
How to speed up Monte Carlo?



Real-time Monte Carlo dose computation will soon be essential for planning and quality assurance of online-adapted treatment plans. By parallelization in GPUs (muscle) and CPUs (brain), this goal is in reach. However, muscle and brain need very specific code optimization for full performance.

Speed and uncompromised accuracy

10x10 mm² field,
6 MeV mono-energetic
point source,
150 mm slab of ICRU-
lung, 0.25 g/cm³
from 50 mm depth.
Blue: SciMoCa,
Red: EGSnrc.



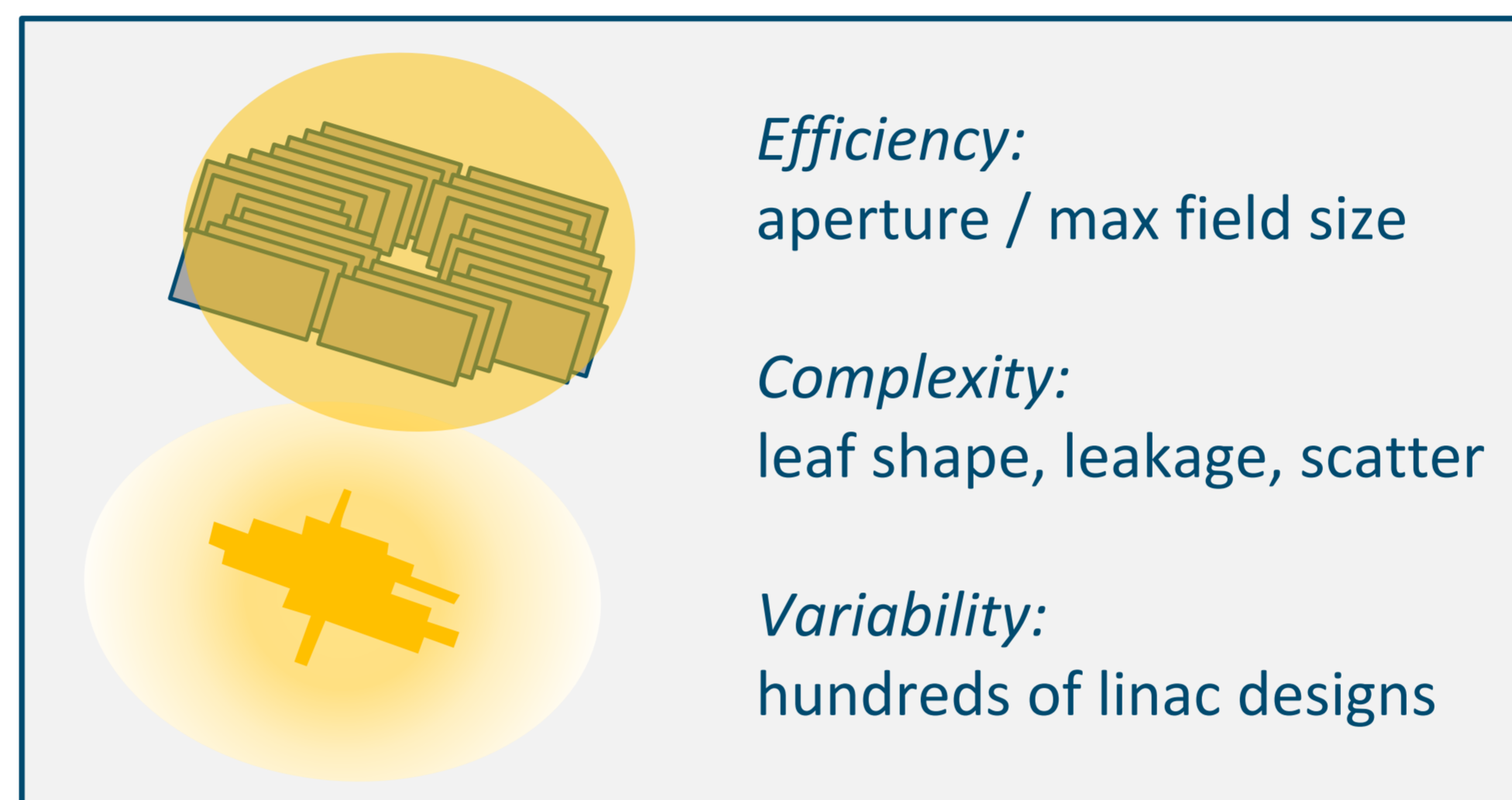
Clinical Monte Carlo:

The accelerator head is crucial for performance

Accelerator head simulations are inherently inefficient:

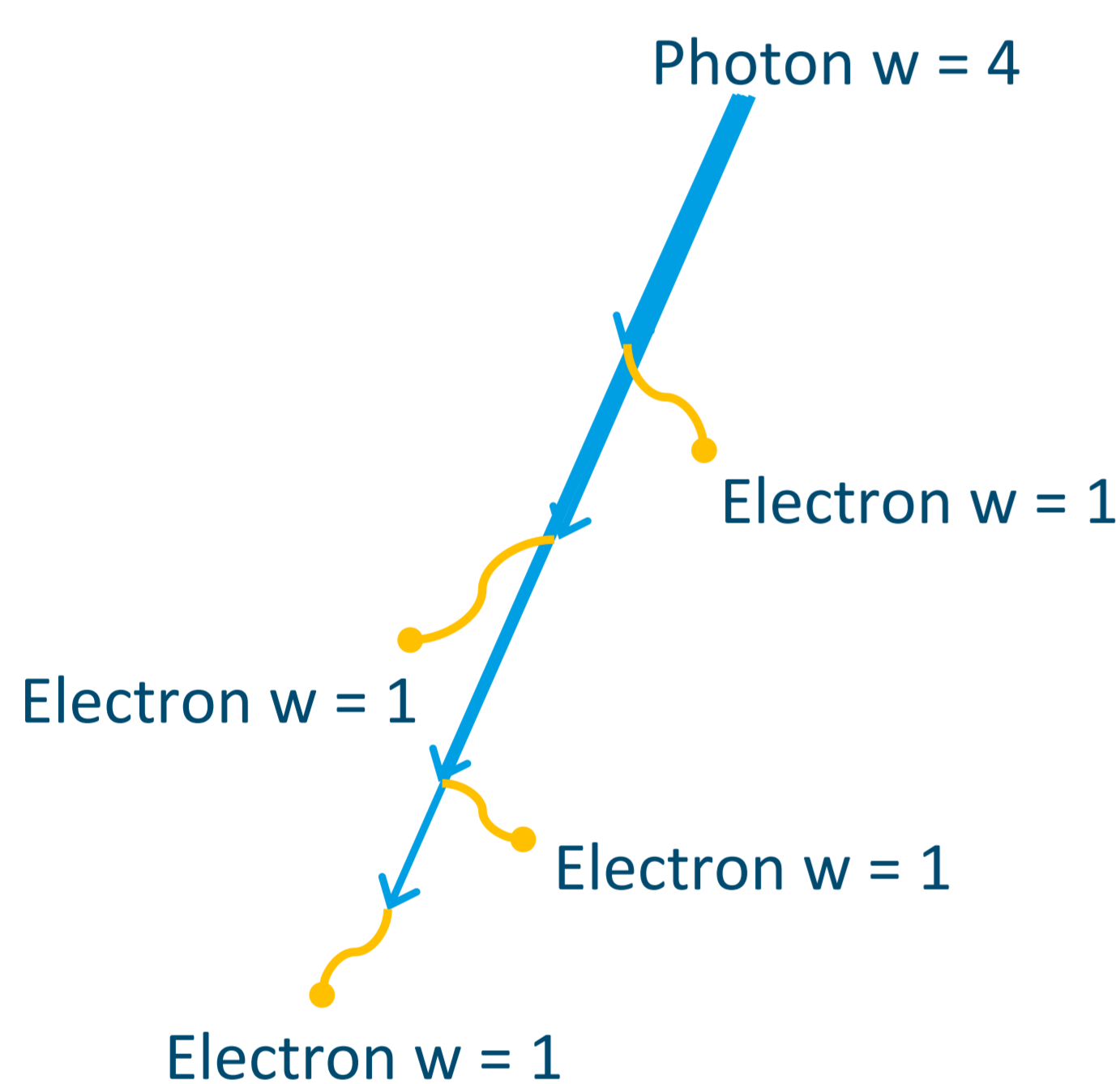
- complex geometries and diverse materials
- many absorbed particles and secondaries
- highly diverse linac designs challenge code optimization

Overall performance is driven by radiation source, collimator model and patient model.



SciMoCa supports all Varian, Elekta, and Siemens linacs, CyberKnife and Tomotherapy:

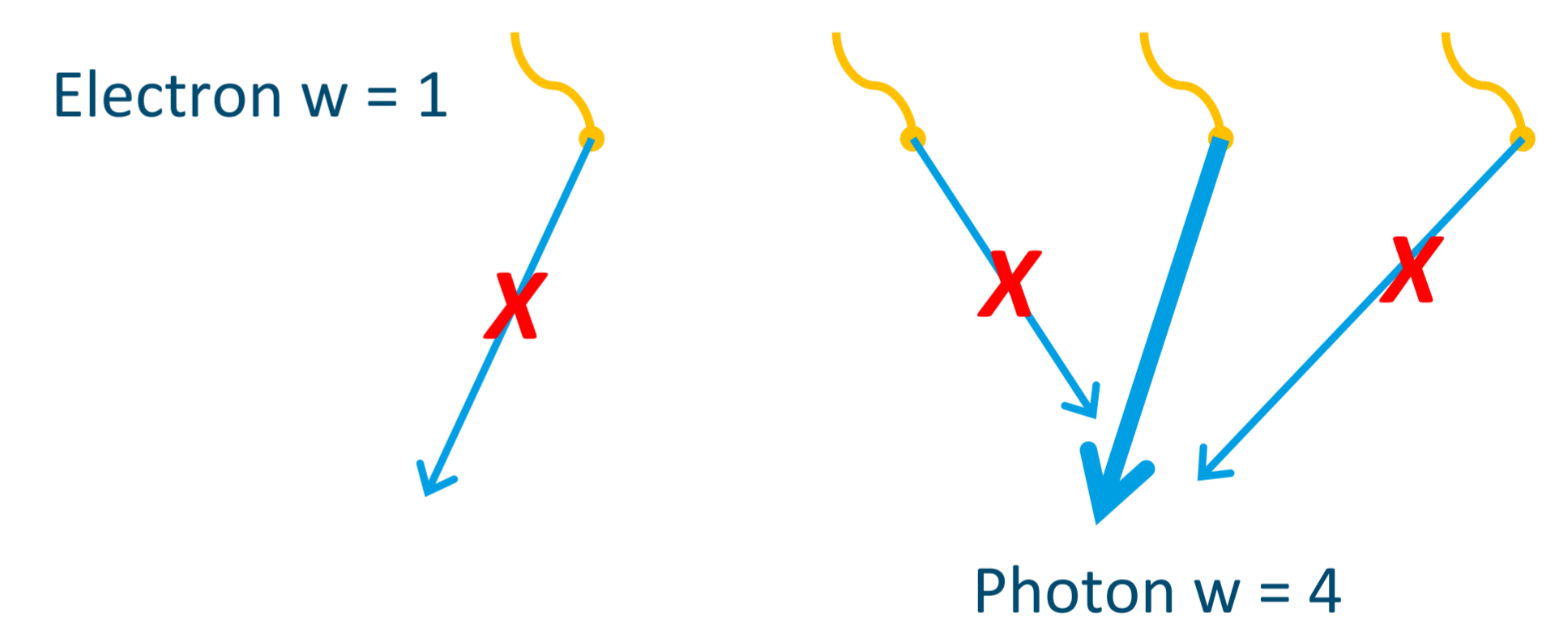
- 16 MLC Types
- 26 Beam qualities
- 41 Flattening Filter designs



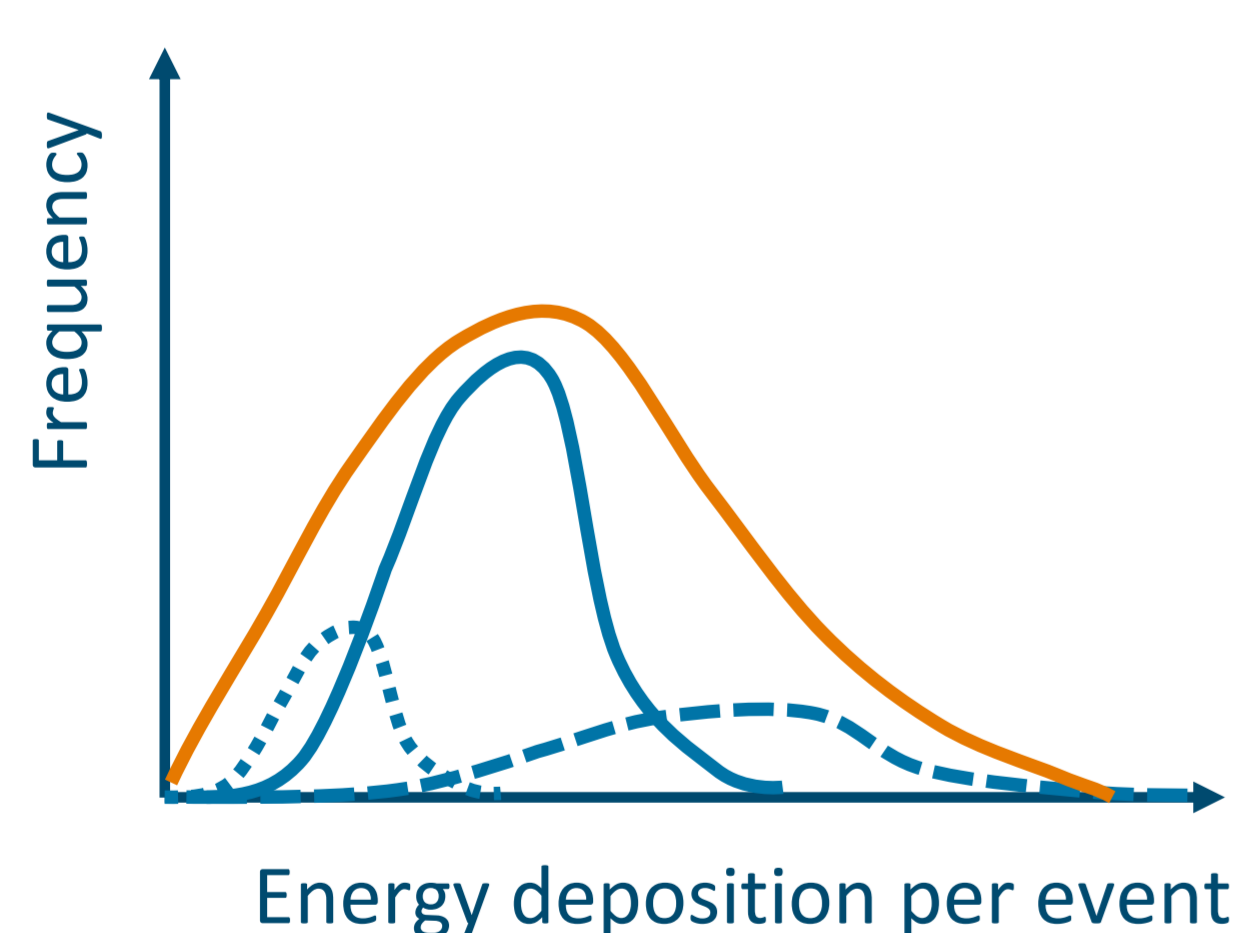
Variance reduction techniques work brilliantly for accelerator heads

Variance reduction techniques utilize statistical particle weights to sample the interactions more efficiently:

- **particle splitting** and history repetition re-use sub-sets of a particle history to save repeat operations
each split reduces particle weight
Example: Photon traverses a leaf
- Russian Roulette discards some less important sub-sets of a particle history and gives higher weight to others
each discard increases particle weight
Example: Photon scatters in flattening filter



The cost of unbalanced particle weight manipulation: convergence efficiency drops



Energy deposition per event in a voxel (tally):
solid line: presumed distribution
dotted, dashed: for particle weights 0.5 and 2
orange: overall tally distribution following VRT

Voxel uncertainty = error of mean

Broadening the tally distribution requires more histories for the same uncertainty

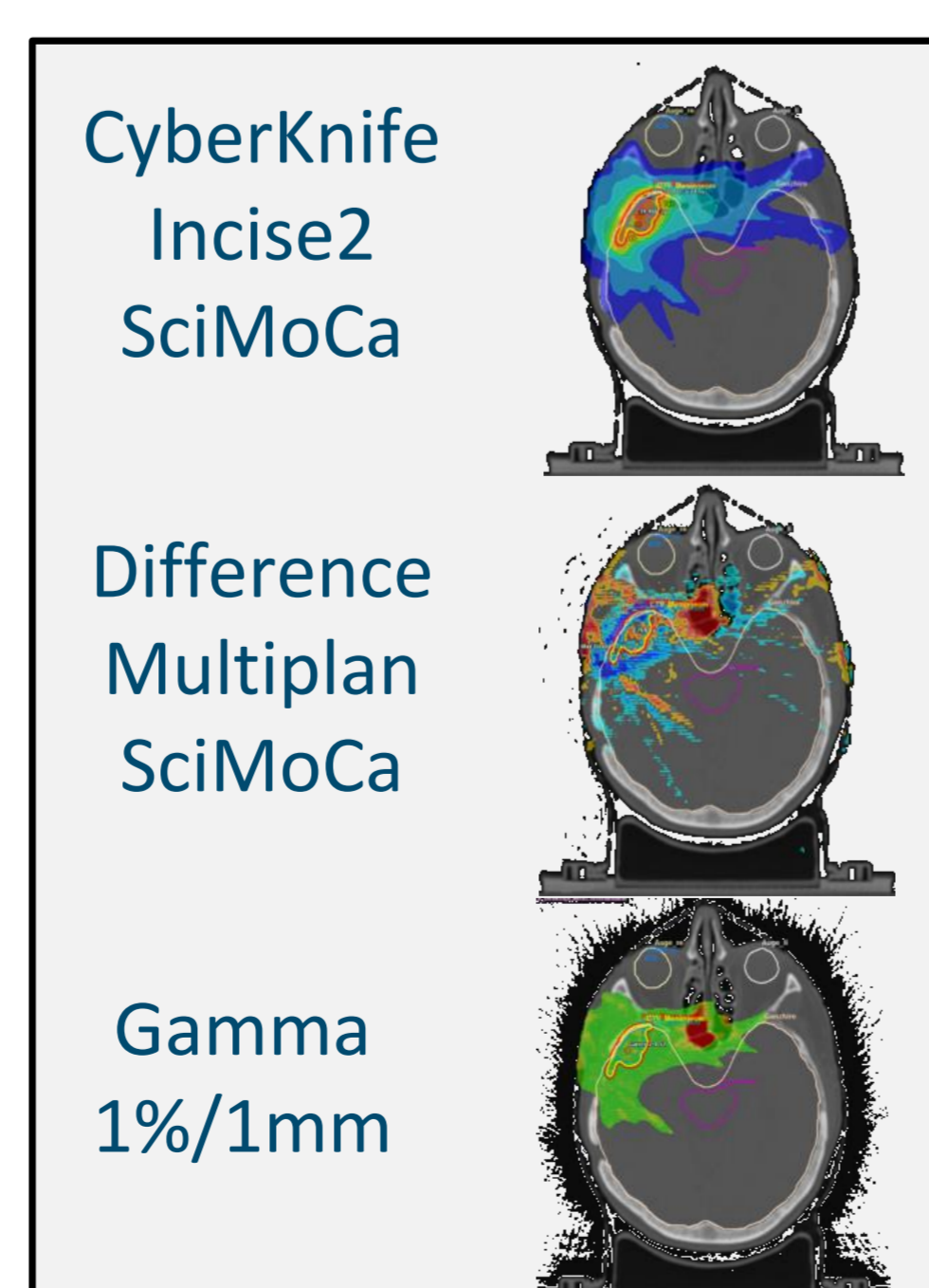
VRT of source- and patient model need to be tuned optimally (case dependent)

Balanced VRT: timings and scaling performance

	prostate, step & shoot (8 beams, 44 segments)	prostate/LN, dMLC (7 beams, 140 control points)	head & neck, VMAT (2 arcs, 293 control points)	
PTV volume	193.3 cc	SIB-case with 2 PTV volumes: 979.8 cc; 159.9 cc	SIB-case with 2 PTV volumes: 834.4 cc; 131.6 cc	
voxel size / uncertainty	3 mm / 1%	3 mm / 1%	3 mm / 1%	2 mm / 1%
calc time 16 cores	15.8 sec	55.6 sec	40.9 sec	118.9 sec
calc time 44 cores	5.6 sec	18.2 sec	14.2 sec	39.3 sec

VRT employed in SciMoCa patient model:

Feature	Value/Reference	Similar to
electron cut-off energy for last Multiple Scatter step	< 240 keV	
fractional energy loss of electron Multiple Scatter step	0.12	
bremsstrahlung production cut-off energy	> 6 keV	
photon cut-off energy (local energy deposit)	< 60 keV	
minimum/maximum particle weight (Russian Roulette ratio)	0.5 < w < 2.0	
maximum photon energy	< 25 MeV	
KERMA-approximation threshold energy	< 1.0 MeV	
Material properties	ICRU 46	XVMC
Material property computation	Kawrakow 1996, Fippel 1999	VMC, XVMC, VMC+
Photon effects	Photoelectric absorption, Compton scatter, Pair production (Kawrakow 2000a)	XVMC, VMC++
Electron effects	Elastic scatter, Møller, Bremsstrahlung (Kawrakow 1996, 2000a)	XVMC, VMC++
Positron effects	Elastic scatter, Bhabha, Bremsstrahlung (Kawrakow 1996, 2000a)	XVMC, VMC++
Multiple Scatter theory	Kawrakow 2000b	EGSnrc, VMC++
Multiple Scatter boundary crossing	Kawrakow 1997, 2001	XVMC, VMC++
Variance reduction techniques	Woodcock tracking, adaptive history repetition, adaptive particle splitting, Russian Roulette, KERMA-approximation	XVMC, VMC++



Fippel 1999: M. Fippel: Med. Phys. 26, 1466 (1999)
Kawrakow 1996: I. Kawrakow, M. Fippel, K. Friedrich: Med. Phys. 23, 445 (1996)
Kawrakow 1997: I. Kawrakow: Med. Phys. 24, 505 (1997)
Kawrakow 2000a: I. Kawrakow, M. Fippel: Phys. Med. Biol. 45, 2163 (2000)
Kawrakow 2000b: I. Kawrakow: Med. Phys. 27, 485 (2000)
Kawrakow 2001: I. Kawrakow in: A. Kling et al. (eds.), *Advanced Monte Carlo for Radiation Physics, Particle Transport Simulation and Applications*, Springer-Verlag Berlin Heidelberg (2001)

Conclusions

Source and collimator simulation increases the complexity of MC:
advantage CPU
VRT tuning causes thread divergence:
advantage CPU
High computational load, low memory access:
high scalability on CPU
Real-time MC is rapidly becoming reality both with GPU and CPU.

